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Differential effects of white matter hyperintensities and regional amyloid deposition on regional cortical thickness



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ABSTRACT

White matter hyperintensities (WMH) and β -amyloid (A β) accumulation have both been linked to neurodegeneration in Alzheimer's disease (AD). However, the independent effects of global WMH and regional A β on the corresponding regional cortical thickness have not been investigated. Here, we evaluated 280 cognitively normal (CN), 450 mild cognitive impairment (MCI), and 63 individuals with AD dementia separately. In CN individuals, only WMH was associated with lower cortical thickness in fronto-temporal regions, independent of regional A β deposition in the corresponding cortical regions. In MCI individuals, the spatial pattern of independent WMH associations was predominantly in temporal and cingulate regions, while independent regional A β associations were now evident in temporal regions. No regional interactions were found. In non-demented individuals and MCI individuals alone, we found that global WMH, composite regional A β burden and cortical thickness in AD-associated regions all independently predicted progression to AD dementia. Our findings suggest that the independent effects of global WMH and regional A β on regional cortical thickness are spatially different, converging in temporal regions in MCI individuals.

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1. Introduction

There has been greater appreciation that mixed dementia is the norm, with Alzheimer's disease pathology most likely to be found alongside another neurodegenerative and vascular pathology, or with at least one vascular pathology (Boyle et al., 2018). Aligning with these pathological evidence, studies have

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sought to establish the independent and interactive effects of ADassociated β -amyloid (A β) burden and white matter hyperintensities (WMH) of presumed vascular origins on magnetic resonance imaging (MRI) measures of neurodegeneration (Bos et al., 2017; Parker et al., 2020; Yassi et al., 2020). While the relationship between WMH and neurodegeneration both cross-sectionally (Du et al., 2005; Habes et al., 2016; Vipin et al., 2018) and longitudinally (Dadar et al., 2022; Kim et al., 2020; Lao and Brickman, 2018; Rizvi et al., 2021) are well-established, the relationships between global WMH, regional $A\beta$ accumulation and regional neurodegeneration are not well understood (De Guio et al., 2020). This may be due to the usage of cerebrospinal fluid (CSF) measures of A β which does not allow for regional analyses or the usage of a global assessment of A β positron emission tomography (PET) standard uptake value ratio (SUVR) or binary positivity to quantify $A\beta$ burden in the brain.



Data used in preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (adni.loni.usc.edu). As such, the investigators within the ADNI contributed to the design and implementation of ADNI and/or provided data but did not participate in analysis or writing of this report. A complete listing of ADNI investigators can be found at: http://adni.loni.usc.edu/wpcontent/uploads/how_to_apply/ADNI_Acknowledgement_List.pdf

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CN(n = 200)	(n = 64)	
Age, M \pm SD 73.37 (6.24) Education, M \pm SD 16.45 (2.64) Sex, Female (%) 154 (55.00) Racial category, White (%) 253 (90.36) APOE e4 dosage (0/1/2) 195/78/7 Log WMH volume, M \pm SD 1.03 (1.10) Florbetapir SUVR, M \pm SD 1.11 (0.18) Cortical Thickness in AD 2.74 (0.13)	$\begin{array}{rrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrr$	

Table 1 Demographics.

Key: AD, Alzheimer's disease; WMH, White matter hyperintensity; SUVR, Standard uptake value ratio.

Given the confluence of evidence showing the presence of amyloid staging regional patterns (Grothe et al., 2017; Mattsson et al., 2019; Pfeil et al., 2021) alongside known regional vulnerabilities to AD-associated neurodegeneration in select cortical regions (Dickerson et al., 2009; Schwarz et al., 2016), regional analyses may provide additional information beyond global assessment of $A\beta$ burden and/or neurodegeneration. Further, it is unknown if these regional spatial relationships are similar across disease stages. Therefore, the current study takes a regional approach by investigating the differential effects i.e., independent contributions and interactive effects of global WMH and regional amyloid PET deposition on the corresponding regional cortical thickness in cognitively normal (CN) individuals, individuals with mild cognitive impairment (MCI), and individuals with AD dementia separately. In addition, while global WMH has been found to be associated with greater progression to dementia (Benedictus et al., 2015; Heng et al., 2021; Kim et al., 2015), whether global WMH, regional A β burden and regional neurodegeneration all contribute independently to clinical progression are unknown.

In sum, using a series of regional and survival analyses, this study aims to determine 1) the differential contribution (i.e., the independent and interaction effects) of global WMH and regional cortical $A\beta$ deposition on regional cortical thickness in CN, MCI, and AD dementia individuals separately and 2) the independent effects of global WMH, composite regional $A\beta$ and cortical thickness in AD-associated regions on progression to AD dementia in non-demented individuals.

2. Methods

2.1. Participants and clinical characterization

Data used in the preparation of this article were obtained from the ADNI database (adni.loni.usc.edu). The ADNI was launched in 2003 as a public-private partnership, led by Principal Investigator Michael W. Weiner, MD. The primary goal of the ADNI has been to test whether serial MRI, PET, other biological markers, and clinical and neuropsychological assessment can be combined to measure the progression of mild cognitive impairment (MCI) and early Alzheimer's disease. Here, we evaluated 280 cognitively normal (CN) individuals, 450 individuals with MCI, and 64 individuals with AD dementia as determined by a global Clinical Dementia Rating (CDR) of 0, 0.5 and \geq 1 respectively. Only participants who had complete white matter hyperintensity, florbetapir SUV, and cortical thickness data that were already processed and available from the ADNI database were included in the study. The resultant sample who had all available data were all from ADNIGO/2. Sample demographics are summarized in Table 1.

2.2. Neuroimaging acquisition and processing

In brief, structural MRI scans were acquired using a 3T scanner. Cortical reconstruction and volumetric segmentation were performed with the Freesurfer 5.1 image analysis suite, which is documented and freely available for download online (http://surfer.nmr.mgh.harvard.edu). The technical details of the procedure have previously been described (Dale et al., 1999; Fischl and Dale, 2000). Regional cortical thickness measures were delineated based on the Desikan-Killany atlas (Desikan et al., 2006) and estimated intracranial volume (ICV) data were also derived using the Freesufer analytic pipeline.

The WMH data were derived from the segmentation of 3D T1 and T2-FLAIR sequences using a Bayesisan approach. FLAIR inhomogeneity corrections were implemented using a histogram normalizing method (DeCarli et al., 1996) and all image segmentations were done in a common template space (DeCarli et al., 2005). Only global WMH data were available in the ADNI database for analyses in the current study.

Florbetapir (18F-AV45) PET images data were co-registered, averaged, interpolated and smoothed. This was followed by coregistration with their 3D T1 that has been processed with Freesurfer 7.1.1 to delineate and compute regional florbetapir SUVRs in cortical regions based on the Desikan-Killany atlas (Desikan et al., 2006). The processing steps of the florbetapir scans have been previously described in greater detail (Landau et al., 2013; Landau et al., 2012).

2.3. Statistical analysis

First, we used linear regression to investigate the basic relationships between global WMH and regional $A\beta$, controlling for age, sex, education, categorical APOE e4 dosage, and estimated ICV. The white matter hyperintensities volume were log-transformed prior to statistical analysis due to non-normality of the distribution (Tan et al., 2019). Regional florbetapir (PET ¹⁸F-AV45) SUVRs were obtained by averaging left and right hemispheres' SUVs in 34 cortical regions of interests (ROIs) derived from the Desikan-Killiany Freesurfer atlas (Desikan et al., 2006) and the averaged SUV in each cortical region was then normalized by the whole cerebellum florbetapir SUV. Next, we investigated the independent i.e., additive contribution of global WMH and regional $A\beta$ on the corresponding regional cortical thickness, controlling for the same covariates. WMH and regional $A\beta$ were used as predictors, regional cortical thickness as criterion variables. The corresponding 34 regional Freesurfer cortical thickness were also obtained by averaging thickness measures for the left and right hemispheres. We cor-



Fig. 1. Independent associations of (A) WMH and (B) regional amyloid SUVR on regional cortical thickness in cognitively normal individuals and (C & D) for individuals with mild cognitive impairment (q < 0.05). No statistically significant associations were found in individuals with AD dementia.

Table 2

Independent associations of white matter hyperintensity and regional amyloid SUVR on regional cortical thickness in cognitively normal individuals.

Region of Interest (ROI)	White Matter Hyperintensity		Florbetapir SUVR		
	Beta	FDR-adjusted q	Beta	FDR-adjusted q	
Banks of the superior temporal sulcus	-0.120	0.097	-0.019	0.837	
Caudal anterior cingulate	-0.131	0.071	-0.093	0.302	
Caudal middle frontal	-0.188	0.013	0.112	0.207	
Cuneus	0.000	0.996	0.030	0.821	
Entorhinal	-0.062	0.376	0.077	0.447	
Fusiform	-0.112	0.105	0.035	0.748	
Inferior parietal	-0.152	0.032	0.060	0.572	
Inferior temporal	-0.123	0.087	-0.111	0.207	
Isthmus cingulate	-0.107	0.128	-0.093	0.302	
Lateral occipital	-0.118	0.093	0.071	0.447	
Lateral orbitofrontal	-0.201	0.009	0.051	0.644	
Lingual	-0.124	0.079	0.134	0.147	
Medial orbitofrontal	-0.083	0.248	0.053	0.644	
Middle temporal	-0.185	0.010	-0.014	0.843	
Parahippocampal	-0.084	0.248	-0.045	0.674	
Paracentral	-0.016	0.848	0.124	0.193	
Pars opercularis	-0.180	0.016	0.020	0.837	
Pars orbitalis	-0.166	0.022	0.017	0.837	
Pars triangularis	-0.186	0.014	0.019	0.837	
Pericalcarine	0.029	0.729	-0.018	0.837	
Postcentral	-0.006	0.952	0.141	0.147	
Posterior cingulate	-0.100	0.178	-0.027	0.837	
Precentral	-0.109	0.123	0.139	0.147	
Precuneus	-0.077	0.273	0.046	0.674	
Rostral anterior cingulate	-0.093	0.205	0.062	0.572	
Rostral middle frontal	-0.205	0.009	0.123	0.193	
Superior frontal	-0.216	0.007	0.118	0.193	
Superior parietal	-0.020	0.810	0.138	0.147	
Superior temporal	-0.164	0.014	0.086	0.302	
Supramarginal	-0.213	0.007	0.135	0.147	
Frontal pole	-0.065	0.375	0.079	0.447	
Temporal pole	-0.166	0.022	0.154	0.147	
Transverse temporal	-0.091	0.205	0.117	0.193	
Insula	-0.214	0.009	-0.003	0.958	

Bold = FDR-adjusted q < 0.05

rected for multiple comparisons at a false discovery rate (FDR) of q < .05 based on a total of 34 linear regressions conducted in all ROIs. Predictors and criterion variables were centered and scaled prior to analysis.

For interaction analyses, we tested whether the interaction of global WMH with regional $A\beta$ was associated with regional cortical thickness. In addition, we derived composite cortical thickness and composite $A\beta$ measures by averaging them in known AD-associated regions (entorhinal, para-hippocampus, inferior parietal,

pars opercularis, pars orbitalis, pars triangularis, inferior temporal, temporal pole, precuneus, supramarginal gyrus, superior parietal, and superior frontal cortex (Dickerson et al., 2009)). We then tested whether there was an interaction between global WMH and composite $A\beta$ on composite cortical thickness. These interaction analyses included all base terms and covariates (age, sex, education, categorical APOE e4 dosage, and ICV). All analyses were conducted separately in the 3 diagnostic groups i.e., CN, MCI and individuals with AD dementia.

Table 3

Independent associations of white matter hyperintensity and regional amyloid SUVR on regional cortical thickness in mild cognitively impaired individuals.

Region of Interest (ROI)	White Matter Hyperintensity		Florbetapir SUVR	
	Beta	FDR-adjusted q	Beta	FDR-adjusted q
Banks of the superior temporal sulcus	-0.203	1.06E-03	-0.220	1.54E-04
Caudal anterior cingulate	-0.105	1.09E-01	0.057	4.73E-01
Caudal middle frontal	-0.087	1.76E-01	-0.070	4.39E-01
Cuneus	0.092	1.76E-01	-0.050	5.02E-01
Entorhinal	-0.119	5.57E-02	0.056	4.51E-01
Fusiform	-0.176	2.13E-03	-0.203	1.79E-04
Inferior parietal	-0.033	6.11E-01	-0.190	1.72E-03
Inferior temporal	-0.143	1.77E-02	-0.240	5.84E-05
Isthmus cingulate	-0.146	1.77E-02	-0.094	1.93E-01
Lateral occipital	-0.032	6.11E-01	-0.162	4.36E-03
Lateral orbitofrontal	-0.226	7.09E-04	-0.056	4.73E-01
Lingual	-0.050	4.42E-01	-0.130	2.85E-02
Medial orbitofrontal	-0.058	3.88E-01	-0.086	3.22E-01
Middle temporal	-0.139	2.05E-02	-0.228	1.03E-04
Parahippocampal	-0.099	1.27E-01	0.044	5.73E-01
Paracentral	0.130	5.01E-02	0.001	9.78E-01
Pars opercularis	-0.046	4.93E-01	-0.034	6.98E-01
Pars orbitalis	-0.189	2.13E-03	-0.060	4.51E-01
Pars triangularis	-0.067	2.98E-01	0.011	9.12E-01
Pericalcarine	0.100	1.30E-01	-0.020	8.46E-01
Postcentral	-0.017	7.67E-01	0.027	7.71E-01
Posterior cingulate	-0.018	7.67E-01	-0.064	4.51E-01
Precentral	0.037	5.68E-01	0.065	4.39E-01
Precuneus	0.012	8.16E-01	-0.183	2.95E-03
Rostral anterior cingulate	-0.153	1.77E-02	0.003	9.78E-01
Rostral middle frontal	-0.082	2.20E-01	-0.017	8.51E-01
Superior frontal	-0.069	2.80E-01	-0.038	6.56E-01
Superior parietal	0.076	2.56E-01	-0.020	8.46E-01
Superior temporal	-0.174	2.13E-03	-0.085	2.23E-01
Supramarginal	-0.126	5.01E-02	-0.061	4.51E-01
Frontal pole	-0.027	6.89E-01	-0.003	9.78E-01
Temporal pole	-0.117	5.97E-02	0.116	6.25E-02
Transverse temporal	-0.114	7.00E-02	0.038	6.54E-01
Insula	-0.218	7.51E-04	-0.017	8.51E-01

Bold = FDR-adjusted q < 0.05

Lastly, we investigated the independent effects of global WMH, composite $A\beta$, and composite cortical thickness on progression to AD dementia using Cox proportional hazards model with time to event indicated by age of AD dementia onset (Tan et al., 2017). We resolved 'ties' using the Breslow method and covaried for age, sex, education, APOE e4 dosage, ICV. We additionally covaried for ICV stratified into quartiles (Tan et al., 2018) to adjust for violations of Cox proportional hazards assumptions by ICV. Conclusions were unchanged regardless of whether this additional covariate was included. None of the variables in the final survival analysis models violated the Cox proportional hazards assumption as determined using scaled Schoenfeld residuals. Due to low conversion rates (n = 5) to AD dementia for CN individuals, these survival analyses were only conducted in all non-demented individuals (CN and MCI together) and in MCI individuals alone. All statistical analyses were conducted using R 4.1.0.

3. Results

3.1. Basic relationships between WMH and regional $A\beta$

In CN individuals, global WMH was associated with A β SUVR in 22 out of 34 regions at uncorrected p < 0.05 (Supplemental Figure 1). These associations were strongest in frontoparietal regions such as the superior frontal, superior parietal, precuneus, postcentral, cuneus, and inferior parietal cortices. However, none of these regions survived multiple correction at FDR-adjusted q < 0.05 (Supplemental Table 1). In MCI individuals, WMH was only associated with superior parietal cortex ($\beta = 0.10, p < 0.05$) but this association also did not survive correction for multiple comparisons. No

associations were found even at uncorrected p < 0.05 for individuals with AD dementia.

3.2. Independent effects of WMH and regional $A\beta$ on regional cortical thickness

In CN individuals, higher WMH volume was significantly associated with lower regional cortical thickness in 13 out of the 34 ROIs (Fig. 1A, Table 2), corrected for multiple comparisons at FDR-adjusted q < 0.05, even after accounting for the corresponding regional $A\beta$ and other covariates. The effects were found predominantly in fronto-temporal regions. In comparison, none of the regional $A\beta$ s were associated with the corresponding regional cortical thickness in the same model containing WMH and other covariates (Fig. 1B, Table 2).

In MCI individuals, the number of regions that higher WMH was independently associated with cortical thickness was reduced to 10 of 34 ROIs (Fig. 1C, Table 3), also corrected for multiple comparisons at FDR-adjusted q < 0.05. The frontal associations were no longer statistically significant while the associations with temporal regions persisted. In addition, WMH associations with regions in the cingulate cortex emerged in these MCI patients. In the same model, higher regional $A\beta$ s were now independently associated with lower cortical thickness in 8 corresponding ROIs (Fig. 1D, Table 3). These associations were strongest in the temporal regions and were also found in regions such as the precuneus and inferior parietal regions. In individuals with AD dementia, WMH was not independently associated with regional cortical thickness in all regions. Although $A\beta$ SUVR was independently associated with cortical thickness in 4 regions (fusiform, supramarginal, precuneus, and

postcentral cortex) at uncorrected p < 0.05, no statistically significant associations were found at FDR-adjusted q < 0.05 (Supplemental Table 2).

3.3. Interactions of WMH and regional $A\beta$ on regional cortical thickness

In all diagnostic groups, there was no evidence of any interactions between WMH and regional A β on regional cortical thickness (FDR-adjusted q > 0.05). We also did not find a significant interaction of WMH with composite A β on composite cortical thickness for CN ($\beta = 0.006$, SE = 0.062, p > 0.05), MCI ($\beta = 0.012$, SE = 0.044, p > 0.05), and individuals with AD dementia ($\beta = 0.244$, SE = 0.154, p > 0.05).

3.4. Independent effects of WMH, $A\beta$ and cortical thickness on progression to AD dementia

In non-demented individuals, 116 individuals (5 CN and 111 MCI) progressed to AD dementia. Higher WMH (Hazard ratio (HR) = 1.39, 95% CI = 1.11 – 1.73), higher composite A β SUVR (HR = 2.74, 95% CI = 2.23 – 3.36), and lower composite thickness (HR = 2.58, 95% CI = 2.11 – 3.56) predicted progression to AD dementia. Similarly, in MCI individuals only, higher WMH (HR = 1.36, 95% CI = 1.09 – 1.70), higher composite A β SUVR (HR = 2.71, 95% CI = 2.15 – 3.43), and lower composite thickness (HR = 2.31, 95% CI = 1.84 – 2.90) all predicted progression to AD dementia.

4. Discussion

The findings presented in the current study supports the differential spatial effects of WMH and regional $A\beta$ burden on regional cortical thickness in CN and MCI individuals, and that WMH are independently associated with progression to AD dementia beyond regional cortical $A\beta$ and neurodegeneration. In CN individuals. greater global WMH was associated with lower regional cortical thickness in predominantly fronto-temporal regions, independent of regional cortical $A\beta$ burden. Although previous studies have reported fronto-temporal associations of WMH and cortical thickness in non-demented individuals without accounting for $A\beta$ burden (Tuladhar et al., 2015), here we additionally show that this fronto-temporal pattern of association is not only independent of fronto-temporal cortical A β accumulation, but also specific to CN individuals only. Our analysis in CN and MCI individuals separately revealed that in MCI individuals, the spatial pattern of this independent regional association shifts from a fronto-temporal pattern to one that retains temporal but not frontal regions, and also now includes the emergence of select cingulate (rostral anterior and isthmus) regions. In individuals with AD dementia, none of the regional associations were statistically significant.

The independent associations between cortical thickness in the cingulate and global WMH in MCI individuals have also been found in a prior study involving only cognitively impaired individuals adjusting for global Pittsburgh compound (PiB) retention ratios (Ye et al., 2015) and may reflect the key role of the anterior cingulate cortex (ACC) in the manifestation of neuropsychiatric symptoms (NPS) that are commonly found in individuals with dementia (Lyketsos et al., 2002; Zhao et al., 2016) which have been linked to underlying mixed cerebrovascular and neurodegenerative pathologies, particularly in more severe disease stages (Kan et al., 2022; Misquitta et al., 2020). The isthmus cingulate also has strong structural and functional connections with the default mode network (Zhu et al., 2013) and its association with WMH independent of $A\beta$ in the current study may reflect the damage to structural white matter fibers due to cerebrovascular disease. Our current study

adds to the literature by suggesting that these cingulate associations are independent of regional $A\beta$ and likely only becomes salient in MCI patients, but not in CN individuals.

While higher regional $A\beta$ was not associated with lower regional cortical thickness independent of WMH in CN individuals, these associations surfaced in temporal regions, precuneus, and inferior parietal cortex in MCI individuals. These are well-established AD-associated regions associated with the neurodegenerative process in Alzheimer's disease (Dickerson et al., 2009) and parallels a previous study involving only cognitively impaired individuals using global PiB (Ye et al., 2015). Our additional finding that the presence of associations of WMH but not regional A β with regional cortical thickness in CN individuals are also consistent with longitudinal findings in individuals across the disease spectrum showing that WMH but not CSF A β_{1-42} levels was associated with changes in grey matter volume (Dadar et al., 2020). The convergence of the independent effects of both WMH and regional $A\beta$ burden in the cortical thickness of temporal regions in MCI individuals may reflect that even at mild cognitive impairment stages, neurodegeneration in temporal regions may be influenced by both cerebrovascular and $A\beta$ pathologies. Temporal regions are known to be vulnerable to greater tau accumulation in AD (Ossenkoppele et al., 2016; Sanchez et al., 2021), and while tau and $A\beta$ show distinct patterns of neurodegeneration, the inferior-lateral temporal lobe in particular has been shown to be a convergence zones of both pathologies (Sepulcre et al., 2016). The absence of statistically significant associations in individuals with AD dementia in the current study may also be suggestive of a shift towards tau-mediated neurodegeneration (Ballatore et al., 2007) in later stages of the disease or simply due to the smaller sample size available for analyses. Future studies additionally covarying for regional tau PET accumulation or extensions of studies investigating remote associations of pathologies (Tosun et al., 2017) may further elucidate the regional and spatial effects of cerebrovascular and both AD pathologies on regional neurodegeneration across different disease stages.

Across these regional analyses, we did not find evidence supportive of an interactive relationship between WMH and regional amyloid PET on regional cortical thickness. Interactive relationships were also not found when averaging $A\beta$ and cortical thickness in known AD-associated regions into composite measures. This lack of regional interaction effects in the current study parallels findings from studies using global $A\beta$ burden where interactive effects are weak or absent, especially in CN individuals (Gordon et al., 2015; Parker et al., 2020; Provenzano et al., 2013; Saridin et al., 2020). In line with a systematic review suggesting that $A\beta$ accumulation and WMH are independent processes (Roseborough et al., 2017), our findings additionally suggest that these processes are independent even when investigated at regional levels of $A\beta$ and neurodegeneration across disease stages.

Our longitudinal survival analyses revealed that global WMH, composite $A\beta$ and composite cortical thickness in known ADassociated regions predicted progression to AD dementia in non-demented individuals and in MCI individuals alone. In both analyses, the hazard ratios of $A\beta$ and cortical thickness were of comparable magnitude with each contributing to about 2.5 times higher risk of progression to AD dementia. In addition, although of a smaller magnitude, global WMH also independently contributed to greater risk of disease progression (~1.4 times). Taken together, our findings support the relevance of WMH as a vascular contribution to the AD process. These results builds upon recent findings (Calvin et al., 2020; Lam et al., 2021) suggesting that WMH may be useful as an additional vascular (V) biomarker in the AT(N) framework (Jack et al., 2018). In addition, given that vascular risk factors are largely modifiable, our results support the potential utility of modifying vascular dysfunction through

interventions (Sweeney et al., 2019) to reduce neurodegeneration and slow down progression to AD dementia.

This study is limited by the fact that ADNI participants with a modified Hachinski ischemic score (Rosen et al., 1980) of above 4 were excluded from the study, and therefore the eligible participants do not represent the entire spectrum of cerebrovascular disease severity. However, given that these relationships were still found in the current study suggest that even moderate presence of cerebrovascular disease can contribute significantly to regional neurodegeneration independent of regional A β burden. Although it is also likely that some of the WMH that we see is due to AD pathology resulting in Wallerian degeneration, post-mortem histological evidence suggests that for older controls, white matter lesions in parietal regions are likely due to ischemia and not ADpathology (McAleese et al., 2017). While regional WMH data were not available on ADNI for analysis in the current study and that lesions in the white matter do not map directly to regional cortical A β and thickness measures, prior studies have found that regional WMH in frontal and parietal regions were associated with faster A β accumulation (Moscoso et al., 2020), that parietal WMH predicted progression to AD dementia (Brickman et al., 2015), and having larger posterior WMH volume was strongly associated with cognitive impairment (Garnier-Crussard et al., 2020). These regional WMH findings suggest that delineating gross regional WMH in the different cerebral lobes in future studies may provide further insights into the regional relationships between these neuroimaging biomarkers. In addition, the independent and interactive analyses were conducted cross-sectionally, future studies may be able to further elucidate potential longitudinal relationships of WMH and regional A β accumulation on the progression of regional cortical thinning. In CN individuals, although the associations of global WMH and regional A β did not survive correction for multiple comparisons, future studies may be able to validate these associations, particularly in the fronto-parietal regions where the effect sizes were the largest. Lastly, these results may not be generalizable to other populations as ADNI participants were recruited to reflect a clinical trial cohort, more than 90% of the participants in ADNI are White and with relatively high education levels.

In conclusion, the current study demonstrates that WMH contributes to regional neurodegeneration, independent of regional $A\beta$ accumulation in different spatial regions as a function of clinical diagnosis – from fronto-temporal in CN individuals to temporal and cingulate regions in MCI individuals. In comparison, the independent influence of regional $A\beta$ on regional neurodegeneration is muted in preclinical stages before manifestation in temporal regions in MCI individuals. The independent associations of global WMH beyond regional $A\beta$ and cortical thickness in ADassociated regions on disease progression also supports the importance of cerebrovascular disease in the AD process. Taken together, our combined results suggest the need for a nuanced understanding of the relationships between WMH, $A\beta$ accumulation and neurodegeneration, which may be regional, dynamic, and differ as a function of clinically diagnosed disease stage.

Disclosure statement

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Verification

The manuscript is not under consideration for publication elsewhere, that its publication is approved by all authors and tacitly or explicitly by the responsible authorities where the work was carried out, and that, if accepted, it will not be published elsewhere in the same form, in English or in any other language, including electronically without the written consent of the copyright-holder.

Supplementary materials

Supplementary material associated with this article can be found, in the online version, at doi:10.1016/j.neurobiolaging.2022. 03.013.

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